form of a dovetail relationship of the collar sides. In lieu of a locking mechanism, a straight split in the collar is sufficient according to one embodiment of the invention. It further is within the scope of the present invention to provide positioning holes **48** in collar **26** in which tools can be inserted for handling and manipulating lens **20**.

The present invention further defines a specially configured instrument, for handling and/or compressing the lens, as best shown in FIG. **5**, generally at **50**. Referring thereto instrument **50** is shown to have a forcep type of construction with first and second arms **52, 54** joined at one end **56** and their opposite ends **58, 60** being provided, respectively, with oppositely disposed box-shaped channels **62, 64** configured for holding collar **24** between them. When the collar is positioned between channels **62, 64**, arms **52, 54** can be compressed together to compress the lens into its narrowed shape, as shown in FIG. **4**, and then inserted as illustrated by the arrow in FIG. **6** into an insertion tool **66** and positioned therein as shown in FIG. **7** to be positioned entirely within insertion tool **66** or with its tip extending out from it. In lieu of the pin attachment at end **56** the arms **52** and **54** can be welded together as in conventional forceps.

Insertion tool **66** comprises a rectangular shaped tubular member **68** having oppositely facing channels **70, 72** in which collar **24** is inserted. A slider member **74** of the tool slides in the channels and is configured with a low profile, as best shown in FIG. **8**, to preferably pass entirely underneath haptic loop **26** and directly engage collar **24** for accurate control of the ejection of lens **20** from the tool into the eye. Although depicted in the drawings as being tubular, the preferred configuration of slider member **74** is flat; it is a flat sheet with proximal thumb loop or ring **80** attached to it to fit under haptic **26** and push against collar **24** to thereby move the lens. Insertion tool **66** includes a pair of oppositely placed finger rings **76, 78** on the sides of tubular member **68** and a third finger ring **80** attached to the end of slider member **74** for controlling its sliding movement as best shown by the hand illustrated with phantom lines in FIG. **6**. These rings are similar to the rings on certain hypodermic syringes provided to ease manipulations of them.

Tubular member **68** is a rectangular tube approximately 3.0 mm wide and 0.5 mm high with a central portion of one flat surface **82** (the top) missing. The internal rectangle defined by tubular member **68** may have its sharp corners rounded. Lens **20** held in the surgeon's finger, or in the compressing instrument **50**, is lubricated with VISCOAT or other visco-elastic substance and inserted into the distal (or proximal) end of the tube. (Alternatively the lens can be inserted in an uncompressed state into a modified insertion tool and the tool compresses it, as well as controllably inserts it, as by pushing it through and out a narrowing channel.) The surgeon slides lens **20** to the desired point, either completely within tubular member **68** or with the forward haptic part of the lens extended. The central portion of the top of the tubular member is omitted so that the surgeon can then use an instrument to position lens **20** in the tubular member from above. The upper opening also allows the surgeon to lubricate the lens from above, to position it within the tube, and to lift the haptic of the lens so that the slider member can pass under it.

By ejecting the compressed intraocular lens **20** slowly and controllably into the eye as is possible with insertion tool **66**, the lens resumes its natural shape without "springing open" within the eye and possibly causing injury. Tool **66** can place the lens in the same position as the manual technique employed with current lenses. The lens is manipulated into its remedial position in either the anterior or posterior chambers of the eye. Fluid **30** then is added or withdrawn from bag **28** through needle **34** inserted into the periphery **32** of the bag. Lens **20** is thus quickly, safely and easily inserted through a small incision into the eye and its refractive power adjusted during the implantation surgery and/or at a later time as needed.

From the foregoing detailed description, it will be evident that there are a number of changes, adaptations, and modifications of the present invention which come within the province of those skilled the art. However, it is intended that all such variations not departing from the spirit of the invention be considered as within the scope thereof as limited solely by the claims appended hereto.

What is claimed is:

1. A small incision intraocular lens comprising:

a deformable soft optic,

a collar positioned generally about said soft optic and compressible about an axis thereof to fit through a small incision into the eye and then expandable when in the eye,

an attaching means for attaching said collar to said soft optic,

a haptic means attached to said collar for remedially positioning said soft optic in the eye after having been inserted therein,

said collar being broken so that a first collar side can slide relative to a second collar side when said collar is compressed, and

said collar including a locking means for locking said first and second collar sides together when said collar is in its expanded state.

2. The intraocular lens of claim **1** wherein said haptic means comprises at least two spaced haptics extending out from said collar.

3. The intraocular lens of claim **3** wherein said haptics comprise at least two J-shaped loops.

4. The intraocular lens of claim **2** wherein said haptics comprise at least two flexible, resilient loops attached at their proximal ends to said collar.

5. The intraocular lens of claim **1** wherein said collar is rigid, generally circular and positioned about the periphery of said soft optic.

6. The intraocular lens of claim **1** wherein said collar includes two collar ends which overlap when said collar is compressed and are in generally abutting relation when said collar is in a relaxed state.

7. The intraocular lens of claim **1** wherein said attaching means attaches the inner surface of said collar directly to the outer surface of said soft optic.

8. The intraocular lens of claim **1** wherein said attaching means comprises a welding means.

9. The intraocular lens of claim **1** wherein said attaching means comprises a plurality of attachments spaced about said collar.

10. The intraocular lens of claim **9** wherein said attachments comprise spot welds.

11. The intraocular lens of claim **1** wherein said soft optic has a biconvex configuration.

12. The intraocular lens of claim **1** wherein said soft optic has a thickened perimeter.